

DEVELOPMENT OF THE SIGNAL EQUATION:

- WE WANT TO DEVELOP A MATHEMATICAL DESCRIPTION OF THE MR SIGNAL FROM A 3D SAMPLE TO BE IMAGED.
- ASSUME A UNIFORMLY SENSITIVE RECEIVER COIL OVER THE ENTIRE F.O.V. (BAD ASSUMPTION, BUT OKAY FOR NOW.)
- RECEIVER COIL IS DESIGNED TO DETECT FLUX CHANGES IN TRANSVERSE DIRECTION (M_{xy} , SINCE WE HAVE ORIENTED B_0 IN THE z DIRECTION)

SIGNAL IS THE SUM OF ALL PRECESSING MAGNETIZATIONS IN THE VOLUME. SIMPLISTICALLY:

$$S_r(t) = \int_{\text{VOLUME}} M_{xy}(\vec{r}, t) dV = \iiint_{x,y,z} M_{xy}(x,y,z,t) dx dy dz$$

HOW ARE WE GOING TO REPRESENT $M_{xy}(\vec{r}, t)$?

PHASOR NOTATION:

$$M_{xy}(\vec{r}, t) = \underbrace{M_{xy}^0(\vec{r})}_{\text{INITIAL CONDITION AFTER TR}} e^{-t/T_2(\vec{r})} \underbrace{e^{-i\omega_0 t}}_{\text{PRECESSION TERM (PHASE)}} \Rightarrow M_{xy} \equiv M_x + iM_y$$

WHERE:

$$\boxed{M_{xy}^0(\vec{r}) = M_x^0 + iM_y^0}$$

$$\omega_0 = \gamma B_0$$

WHAT HAPPENS WHEN WE INCLUDE THE EFFECTS FROM GRADIENTS?

- WE SPEED UP OR SLOW DOWN THE PRECESSION (PHASE) TERM!
- IN GENERAL:

$$\boxed{B(\vec{r}, t) = (B_0 + G_x^{(k)}x + G_y^{(k)}y + G_z^{(k)}z) \hat{k} = (B_0 + \vec{G}(t) \cdot \vec{r}) \hat{k}}$$

SO:

$$\boxed{\omega(\vec{r}, t) = \gamma B_0 + \gamma \vec{G}(t) \cdot \vec{r}} = \boxed{\omega_0 + \gamma \vec{G}(t) \cdot \vec{r}}$$

NOW, CAN I SIMPLY PLUG THIS EXPRESSION IN TO MY EXPRESSION FOR $M_{xy}(\vec{r}, t)$??

NO!

PHASE TERM
 MY PHASOR TERM $e^{-i\omega_0 t}$ GIVES THE PHASE AT TIME t . THIS DEPENDS NOT ONLY ON THE CURRENT FREQUENCY $\omega(t)$ BUT ON FREQUENCIES IN THE PAST!

IN FACT:

$$\text{PHASE} = \int_0^t \omega(\vec{r}, \tau) d\tau$$

IN THE CASE WHERE:

$$\omega(\vec{r}, t) = \omega_0$$

WE HAVE:

$$\text{PHASE} = \int_0^t \omega_0 d\tau = \omega_0 t$$

NOW, WHEN $\omega(\vec{r}, t)$ IS TIME VARYING, WE HAVE:

$$\text{PHASE} = \int_0^t \omega(\vec{r}, \tau) d\tau = \int_0^t [\omega_0 + r \vec{G}(\tau) \cdot \vec{r}] d\tau$$

$$\text{PHASE} = \int_0^t \omega_0 d\tau + \int_0^t r \vec{G}(\tau) \cdot \vec{r} d\tau$$

$$\text{PHASE} = \omega_0 t + \int_0^t r \vec{G}(\tau) \cdot \vec{r} d\tau$$

WE CAN PLUG THIS IN WHERE WE SIMPLY HAD $\omega_0 t$ BEFORE:

$$M_{xy}(\vec{r}, t) = M_{xy}^0(\vec{r}) e^{-t/T_2(\vec{r})} e^{-i[\omega_0 t + \int_0^t r \vec{G}(\tau) \cdot \vec{r} d\tau]}$$

$$M_{xy}(\vec{r}, t) = M_{xy}^0(\vec{r}) e^{-t/T_2(\vec{r})} e^{-i\omega_0 t} e^{-i r \int_0^t \vec{G}(\tau) \cdot \vec{r} d\tau}$$

PLUGGING INTO OUR SIGNAL EQUATION, WE HAVE:

$$S_r(t) = \iiint_{x,y,z} M_{xy}^o(x,y,z) e^{-\frac{t}{T_2(z)}} e^{-i\omega_0 t} e^{-i\gamma \int_0^t \vec{G}(\tau) \cdot \vec{r} d\tau} dx dy dz$$

\Rightarrow TO SIMPLIFY,
 WE'RE GOING TO
 IGNORE RELAXATION
 FOR NOW.

\Rightarrow WE ALSO ASSUME SLICE SELECTIVE EXCITATION
 TO GO TO 2D (FROM 3D)

- IF WE TIP THE WHOLE VOLUME UNIFORMLY, THEN:

$m(x,y)$ & $M_{xy}^o(x,y)$ \leftarrow WITH z INTEGRATED
 OVER SLICE WIDTH
 \uparrow
 THE THING
 WE'RE
 IMAGING

so:

$$S_r(t) = \iint_{x,y} m(x,y) e^{-i\omega_0 t} e^{-i\gamma \int_0^t \vec{G}(\tau) \cdot \vec{r} d\tau} dx dy$$

NOW LET'S DEMODULATE OUR SIGNAL AT FREQ. ω_0 :

$$s(t) = S_r(t) e^{+i\omega_0 t}$$

THEN:

$$s(t) = \int_x \int_y m(x,y) e^{-i\gamma \left[\int_0^t x G_x(\tau) d\tau + \int_0^t y G_y(\tau) d\tau \right]} dx dy$$

PUTTING IT ALL TOGETHER, WE CAN WRITE:

$$s(t) = \int_x \int_y m(x,y) e^{-i2\pi [k_x(t)x + k_y(t)y]} dx dy$$

WHERE:

$$k_x(t) = \frac{\gamma}{2\pi} \int_0^t G_x(\tau) d\tau$$

$$k_y(t) = \frac{\gamma}{2\pi} \int_0^t G_y(\tau) d\tau$$

NOTICE THAT $s(t)$ LOOKS A LOT LIKE A ^{2D} FOURIER TRANSFORM!!

IF WE LOOK AT THE FT. OF $m(x,y)$:

$$M(k_x, k_y) = \int_x \int_y m(x,y) e^{-i2\pi(k_x x + k_y y)} dx dy$$

THEN WE SEE THAT:

$$s(t) = M(k_x(t), k_y(t))$$

IN OTHER WORDS, $s(t)$ IS GIVING US THE VALUE OF THE 2D FT OF $m(x,y)$ AT k -SPACE POSITION $(k_x(t), k_y(t))$ AT A GIVEN VALUE OF t !

THIS IS THE BASIS FOR THE VERY POWERFUL "FOURIER INTERPRETATION" OF THE SIGNAL EQUATION.

BY MANIPULATING OUR TIME-VARYING GRADIENTS $G_x(t)$ AND $G_y(t)$ APPROPRIATELY, WE CAN "TRAVERSE" k -SPACE IN ANY WAY WE WANT, AND SAMPLE VALUES OF $M(k_x, k_y)$ FROM THE SIGNAL $s(t)$.

THIS IS VERY POWERFUL, AND THE BASIS FOR MRI PULSE SEQUENCE DESIGN.